Semi-Supervised Generative Adversarial Network (SGAN) for Nuclei Detection on Breast Cancer Histopathology Images

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*Abstract*—We extended work on the SGAN model by combining it with an implemented DCGAN, and by making some adjustments in said model to work with a H&E breast cancer histopathology images dataset published by the Case Western Reserve University. Our goal was to evaluate if the Discriminator (or semi-supervised model) could achieve comparable or better performance to the aforementioned SGAN, which finds the probability that input image patches correspond to (and thus detect) nuclei. Our results showed that our model was able to learn useful high-level features of nuclear structures as well as to generate visually appealing samples. We conclude that more experimentation is necessary to formulate a more robust and significant progression.

Keywords— Feature representation learning; automated nuclei detection; semi-supervised approach; Generative Adversarial Network; breast cancer histopathology.

# Introduction

Nuclei Detection allows researchers to identify each individual cell in a sample. By measuring how cells react to various treatments, the researcher can understand the underlying biological processes at work. The analysis of histopathology images is currently the standard in diagnosing Breast Cancer (BC). This fact is a convincing motivation to discover, enhance, and automated efficient approaches to distinguish individual cancer nuclei on breast pathology images.

Getting large amounts of unlabeled medical data is generally much easier than labeled data. Unsupervised generative models with stochastic components (like GANs and VAEs) can be trained end-to-end to learn representative features in a completely unsupervised way. For that reason, both approaches could optimally leverage this amount of information.

The following is an outline of the rest of this paper. A review of similar architectures and previous related works is presented in Section II, a detailed description of Semi-Supervised Generative Adversarial Network (SGAN) is presented in Section III, the experimental setup and comparative strategies are discussed in Section IV, the experiment results and discussions are reported in Section V, and conclusions and future work are presented in Section VI.

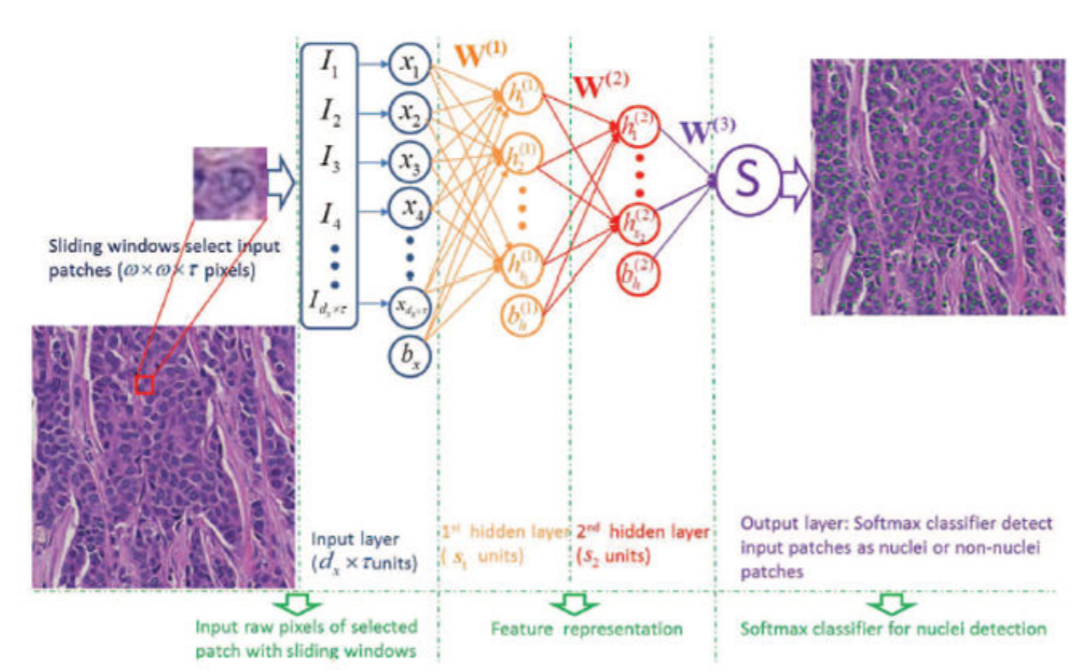


Figure 1. Illustration of SSAE+SMC for nuclei detection on breast histopathology

# Previous Related Work

## Stacked Sparse Autoencoder (SSAE) for Nuclei Detection on Breast Cancer Histopathology Images

An interesting approach, especially in cases where object annotation to generate training data is expensive, is the integration of multiple instance learning (MIL) and deep learning. Xu et al. [1] investigated the use of a MIL-framework with both supervised and unsupervised feature learning approaches as well as handcrafted features (2016). The results demonstrated that the performance of the MIL-framework was superior to handcrafted features, which in turn closely approaches the performance of a fully supervised method.

Training an SSAE+SMC (SMC stands for Softmax Classifier) model involves finding the optimal parameters θ= (W, bh, bx) simultaneously by minimizing the discrepancy between input and its reconstruction. After the optimal parameters θ are obtained, the SSAE+SMC yields a function that transforms input pixel intensities of an image patch to a new feature representation of nuclear structures.

As Fig. 1 shows, with SSAE+SMC, each training patch of pixel intensities is represented by a high-level structured representation of nuclei or non-nuclei patches (2) in the second hidden layer of the model. Note that in the SSAE learning procedure, the label information *y* is not used. Hence, SSAE learning is an unsupervised learning scheme.

During detection process, each image patch detected by a sliding window is first represented by high-level feature (2). This is then fed to the SMC and produces a value between 0 and 1 that can be interpreted as the probability of the input image patch corresponding to a nucleus or not.

Similarly to the SSAE model, our model’s G can transform the input pixel intensities to structured nuclei or non-nuclei representations. Therefore, our GAN based framework is also able to learn high-level structure information from a large number of unlabeled image patches. Although both approaches are generative models and VAE tend to have a clearer and objective cost function, We decided to use a SGAN because (1) unlike VAE, GANs are able to generate more realistic samples and (2) recently published papers revealed effective techniques to produce more stable GANs [17], [5].

## Generative Adversarial Networks (GAN)

GANs are based on a game theoretic scenario in which the generator network must compete against an adversary. The generator network (G) directly produces samples Its adversary, the discriminator network (D), attempts to distinguish between samples drawn from the training data and samples drawn from the generator. The discriminator emits a probability value given by , indicating the probability that is a real training example rather than a fake sample drawn from the model [2].

The representations that can be learned by a GAN may be used in a variety of applications, including image synthesis, semantic image editing, style transfer, image super-resolution, and classification [3]. Expanding these ideas, one can produce good output samples using a set of convolutional neural networks [4]. Some years ago, Radford [5], created surprisingly good samples from a single generator network.

## DCGAN

Several recent papers focus on improving the stability of training and the resulting perceptual quality of GAN samples [6], [7], [8], [9], and [10]. Among these, Radford et al. [5] main contribution came from a set of practices that prove to stabilize the training of GAN by: (1) replacing deterministic spatial pooling functions (such as maxpooling) with strided convolutions, (2) eliminating fully connected layers on top of convolutional features, and (3) not applying Batch Normalization [11] to the generator output layer and the discriminator input layer.

We use some of these architectural innovations proposed in Radford et al. [5], as discussed in Section III.

# SGAN

Odena [12] proposed an extension of the DCGAN architecture to the semi-supervised context by forcing D to output N+1 different output classes, N different “real” classes, and an additional fake class (anything that came from G). In our case, N=2 (real nuclei, and real non-nuclei).

Using generative models on semi-supervised learning tasks is not a new approach. Kingma et al. [13] expand the work on variational generative techniques ([14], [15]) to do just that. However, Odena [12] described a new extension called SGAN that improves classification performance on restricted data sets over a baseline classifier with no generative component.

According to Odena [12], training an SGAN is similar to training a GAN. One simply use higher granularity labels for the half of the minibatch that has been drawn from the data generating distribution. D is trained to minimize the negative log likelihood with respect to the given labels and G is trained to maximize it, as shown in Algorithm 1.

1 SGAN Training Algorithm

|  |
| --- |
| **Input:** I: number of total iterations  **for** **to** I **do**  Draw noise samples from noise prior .  Draw examples from data  generating distribution .  Perform gradient descent on the parameters of D w.r.t. the  NLL of D’s outputs on the combined minibatch of size  .  Draw noise samples from noise prior .  Perform gradient descent on the parameters of G w.r.t. the  NLL of D’s outputs on the minibatch of size *m.*  **end for** |

Our work can be seen as a refinement of this method adapted to perform nuclei detection.

# Experimental Setup

Initially, we conducted experiments on MNIST to see whether the classifier component (D) of our model could perform as intended and similar to the original implementation. Then, we conducted experiments on the TMI Dataset (the Breast Cancer histopathology images).

The experiments in this paper were conducted with [18], which borrows heavily from [19] and contains more details about the experimental setup.

## TMI Dataset

In order to be able to compare the experimental results with the SSAE model, the experimental setup for the dataset was almost identical to Xu et al [1]. We use the same dataset of 537 H&E stained histopathological images, obtained from digitized glass slides corresponding to 49 lymph node-negative and estrogen receptor-positive breast cancer (LN-, ER+ BC) patients at Case Western Reserve University. The training data includes 2,000 nuclear and 6,000 non-nuclear patches. There are 1,000 patches for validation, 500 nuclear patches and 500 non-nuclear. The complete access to the full dataset is provided at Error: Reference source not found. Xu et al [1] explains the generation of the training and ground truth datasets. In this paper, we did not use the testing dataset. Instead we used the validation as the testing dataset.

This dataset already contains the data divided into train and validation. The value range of each image was originally [0…1] but we normalize it to be [-1…1].We modify training and testing labels. 0 represents non-nucleus, 1 represents nucleus.

## Parameter setting

To train the model with the TMI dataset, the patch size was initially defined as pixels. However, due to fact that G input image has to start from a integer number, every image from the training dataset was downscaled to pixels which is big enough to contain a nucleus within the patch under 40X optical magnification resolution images. Each patch size has three color channels (). Therefore, there are input units in the input layer.

Regarding the optimizer, we used the same Odena used [12] Adam optimizer [16] with tuned hyper-parameters. We use 0.0002 as the learning rate, and 0.5 as momentum term , which helped stabilize training. Both, G and D used the same optimizer. Figure 2 and Figure 3 depicts the architecture of both models (very similar to the DCGAN).

We used almost all architecture guidelines suggested by Radford [5] for a stable Deep Convolutional network:

* Replace any pooling layers with strided convolutions (discriminator) and fractional-strided convolutions (generator).
* Use batchnorm in both the generator and the discriminator.
* Remove fully connected hidden layers for deeper architectures.
* Use ReLU activation in generator for all layers except for the output, which uses Tanh.
* Use LeakyReLU activation in the discriminator for all layers.

A notably difference relies on G first layer which is an 8×8×128 this size assures that the generator outputs an image with equal size as the training images.

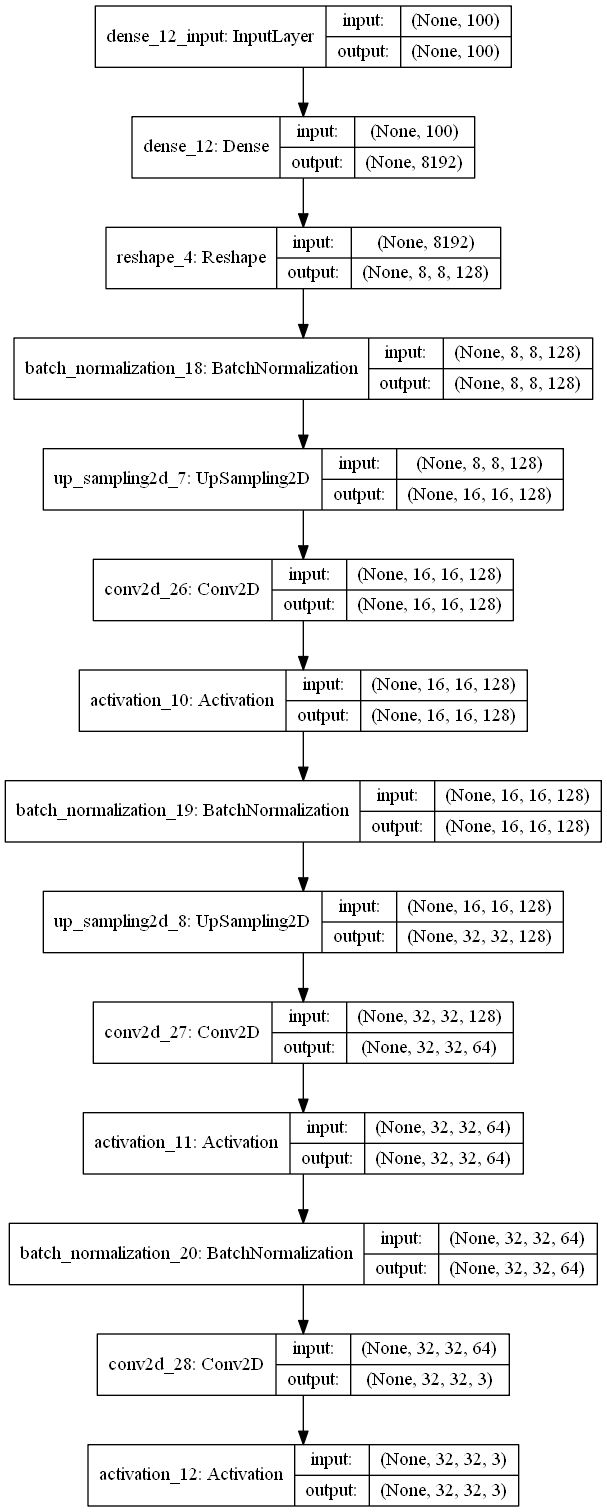


Figure 2. G model’s graph.

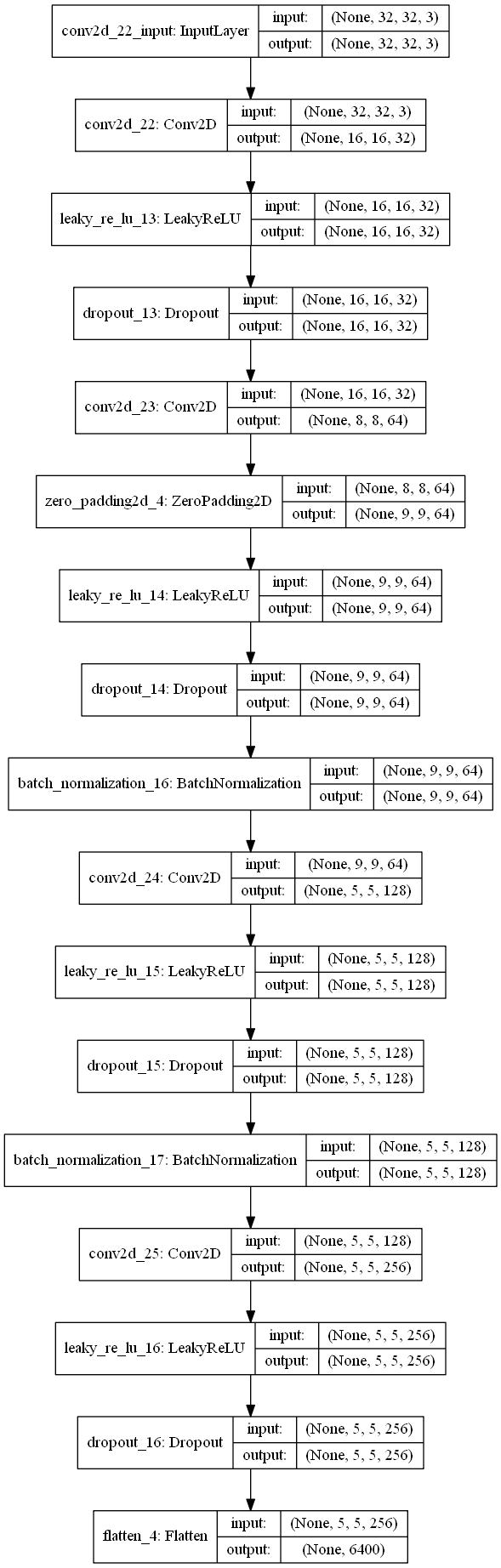


Figure 3. D model’s graph.

## Training the SGAN for Nuclei Detection

The training procedure was for 200 epochs, with a batch size of 32 images. For each epoch, we selected a random half batch of images from the TMI training set (16 images) and another random half samples from a Gaussian distribution. To balance the difference in occurrences of class labels, 50% of labels that the D trains on are “fake”, i.e., class weights were also divided equally. This approach is called by [17] as *Mini-batch discrimination*. SGAN entire training time was 6 minutes and 12 seconds.

### Training the Discriminator (D)

The random half batch of images from a Gaussian distribution are given to G who transform this noise into a set of synthetic images. The goal is to stabilize D learning process by sending send 2 different mini-batches one for real and one for fake images.

The discriminator, now a multi-class classifier, is the most relevant network for this architecture. After a series of convolutions, batch normalization, leaky RELUs and dropout, we instantiate the model with two activation functions. A sigmoid activation function to indicate the predicted probability of the given image being real or fake, and, if and only if the image is real, a softmax activation function with classes to indicate the predicted probabilities of the given image being nucleus (label=1) or non-nucleus (label=0).

D’s is trained by minimizing the cross-entropy between the observed labels and the model predictive distribution .

### Semi-supervised learning for Nuclei Detection

The way D does semi-supervised learning is by adding samples from G to D’s data set, labeling them with a new “generated” class , and correspondingly increasing the dimension of D’s output from to . We then use to supply the probability that a given image *x* is fake (coming from G). With this in mind, we can now learn from unlabeled data, as long as we know that it corresponds to one of the K classes of nuclei data by maximizing .

### Training the Generator (G)

The Generator follows a very standard implementation described in the DCGAN paper. This approach consists of reshaping a random vector z to have a 4D shape and then feed it to a sequence of transpose convolutions, batch normalization and leaky RELU operations that increase the spatial dimensions of the input vector while decreases the number of channels. As a result, the network outputs a 32x32x3 RGB tensor shape that is normalized between values of -1 and 1 through the Hyperbolic Tangent Function (tanh).

G is trained 10 times per epoch to overcome a failure mode in where D overpowered G, classifying generated images as fake with absolute certainty and leaving no gradient for the generator to descend. The number 10 was empirically defined. Fig. 4 shows a randomly generated batch of 25 images per epochs during G’s training phase. Fig. 5 shows D and G accuracy and loss per epoch.

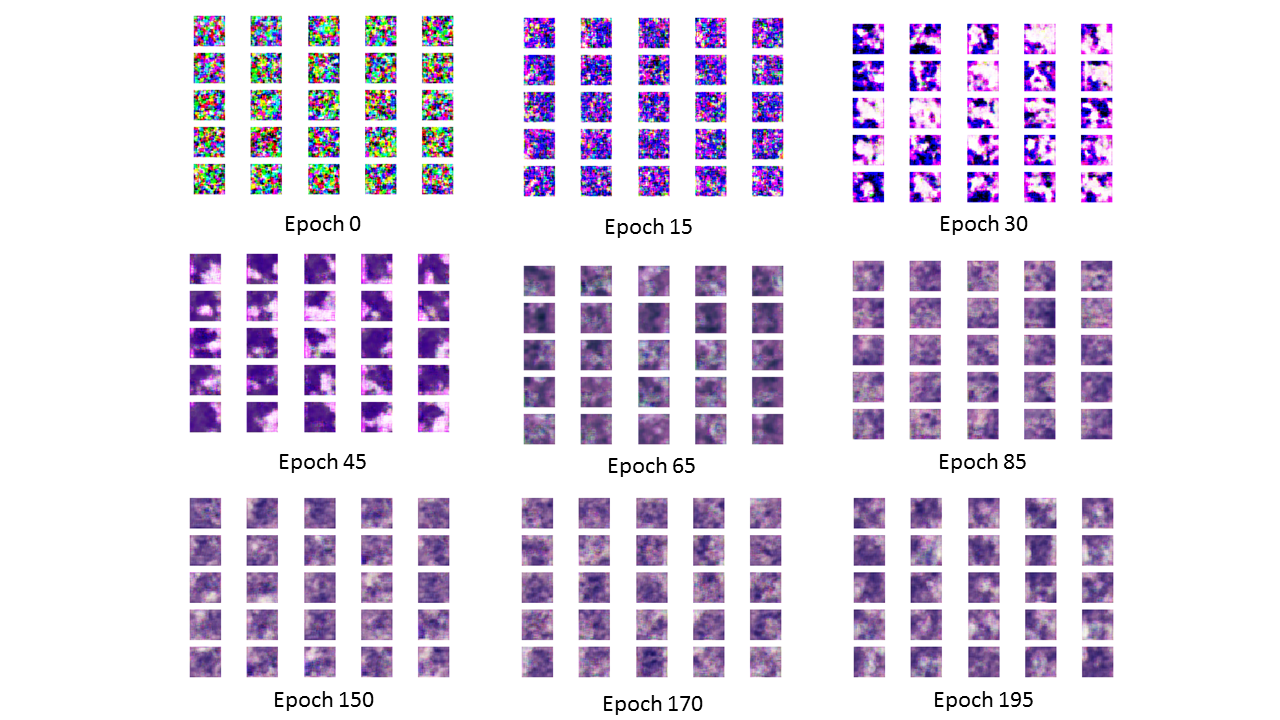


Figure 4. Generator's output per epoch

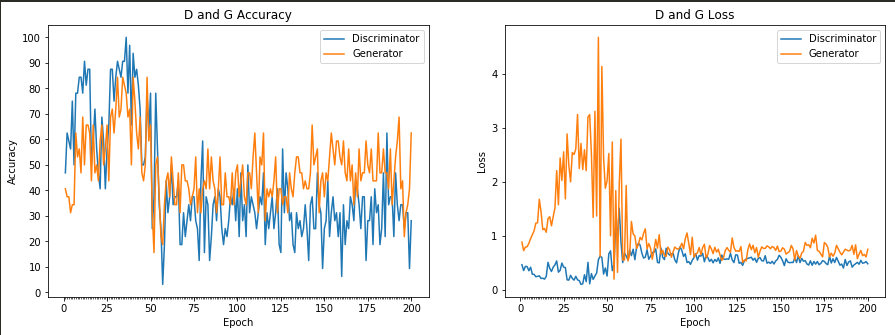


Figure 5. D and G accuracy and loss per epoch

## Experimental design and comparative strategy

In order to show the effectiveness of our model, the model is compared against the state-of-the-art model Stacked Sparse Autoencoder plus Softmax Classifier (SSAE+SMC) [1].

The aim of this experiment was to compare SSAE and SGAN for the problem of nuclei detection.

For SSAE, the detection procedure is the same as illustrated in Figure 1. A sliding window detector is first employed to select image patches before feeding to the model. Then high-level features are extracted via this model and this features are then subsequently input to SMC. Finally, the trained SMC classifies each image patch as either having or not having a nucleus present. Readers can refer to Xu et al. [1] for more details.

## Performance Evaluation

The performance of automatic nuclei detection is quantified in terms of Precision, Recall or True Positive Rate (TPR), False Positive Rate (FPR), F-measure, and Average Precision (AveP).

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However, the definition of each term is different for each approach. Xu et al [1] used the a testing dataset :

True Positive (TP) is defined as the number of nuclei correctly identified as such by the model. In Xu et al. paper, the correct detection of nuclear patches (true positives) was identified as those instances in which the distance between the center of the detected nuclear window and the closest annotated pathologist identified nucleus was less than or equal to 17 pixels.

TP + FN is defined as the total number of automatically detected nuclei. FP+TN is defined as the total number of patches without nuclei.

Average Precision (AveP) involves computing the average value of p(r) over interval between r = 0 and r = 1 and the precision p(r) is a function of recall r. Therefore, AveP shows the average area under Precision-Recall curve.

For our model (SGAN), we did not used the TMI testing set. Instead, we used the entire training set that was already divided into 8,000 samples for training and 1,000 samples for testing. We computed the standard definition of Precision, Recall or True Positive Rate (TPR), False Positive Rate (FPR), F-measure, and Average Precision (AveP) over this dataset.

# Experimental Results

D’s overall classification accuracy across the 1,000 testing was 94.100%. Thus, D’s error rate is 0.59. Figure 6 and 7 shows the confusion matrix (also known as an error matrix) visualize the performance of our SGAN model. What’s notable here about these matrices is that the system makes a highly accurate distinction between nucleus and non-nucleus as values outside the diagonal are very low and balanced.



Figure 6. SGAN Confusion Matrix without normalization



Figure 7. SGAN Normalized Confusion Matrix

We computed the precision, recall, F-measure and support for each class. The precision is the ratio where *tp* is the number of true positives and *fp* the number of false positives. The precision is intuitively the ability of the D not to label as nucleus a sample that is not a nucleus.

The recall is the ratio where tp is the number of true positives and *fn* the number of false negatives. The recall is intuitively the ability of the D to find all the nucleus samples.

The F-measure can be interpreted as a weighted harmonic mean of the precision and recall, where an F-measure score reaches its best value at 1 and worst score at 0. In this case, F-measure was not weighed *w.r.t.* any factor, i.e. . Table 2 shows a classification report for our SGAN’s D model.

The SSAE-SMC model [1] used a different approach and dataset to calculate its Precision, Recall, F-measure and Average Precision (*AveP*). However, the classification task was somehow similar, due to the fact that both model (the SSAE and SGAN) output the probability of the input image patch corresponding to a nucleus or not through a Softmax Classifier. That is why we considered pertinent to compare its values in Table 3.

Table 2. SGAN’s D Classification Report

|  |  |  |  |  |
| --- | --- | --- | --- | --- |
|  | **Precision (%)** | **Recall (%)** | **F-measure (%)** | **Support (%)** |
| Non-Nucleus | 95 | 93 | 94 | 500 |
| Nucleus | 93 | 95 | 94 | 500 |
| Avg / Total | 94 | 94 | 94 | 1000 |

Table 3. The mean associated with Precision, Recall, F-measure and Average Precision (AveP) for SSAE+SMC, and SGAN’s D

|  |  |  |  |  |
| --- | --- | --- | --- | --- |
| **Model** | **Precision (%)** | **Recall (%)** | **F-measure (%)** | **AveP (%)** |
| SSAE-SMC | 88.84 | 82.85 | 84.49 | 78.83 |
| SGAN | **94** | **94** | **94** | **93.2** |

# Conclusion and future work

In this paper, a Semi Supervised Generative Adversarial Network (SGAN) is presented for automated nuclei detection on breast cancer histopathology. We have shown how the model can capture high-level feature representations of pixel intensity in a semi-supervised manner. These high-level features enable the classifier to work very efficiently for detecting multiple nuclei from a large cohort of histopathological images as well as to generate realistic synthesized representations of nuclei and non-nuclei images. To show the effectiveness of the proposed framework, we compared it with the SSAE model [1]. Regardless of the difference in the testing approach and dataset that both models used, the SGAN model appear to suggest that it works well in learning useful high-level features for better representation of nuclear structures. However, these evaluations are not enough to conclude that it can outperform state-of-the-art methods on nuclei detection.

We are eager to explore the following related ideas to improve our results and arrive to a more certain conclusion:

* Replicate the testing procedure from Xu et al. [1]. And implement the same qualitative, quantitative and sensitivity analysis to have a better intuition when comparing both models.
* Improve SGAN model training by evaluating the impact of recently published techniques such as: One side label smoothing, Historical averaging, Virtual Batch Normalization (VBN), and Inception Scoring proposed by Salimans et al. [17], Feature Matching [17] and [20], Adding some artificial noise to inputs [22] and [22].

##### Acknowledgment

Class of Computer Vision.

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